

Topologic and Geometric Approaches for In Vivo Quantitative Assessment of Trabecular Bone Micro-Architecture

Punam Kumar Saha
Professor
Departments of ECE and Radiology
University of Iowa
pksaha@engineering.uiowa.edu

Overview

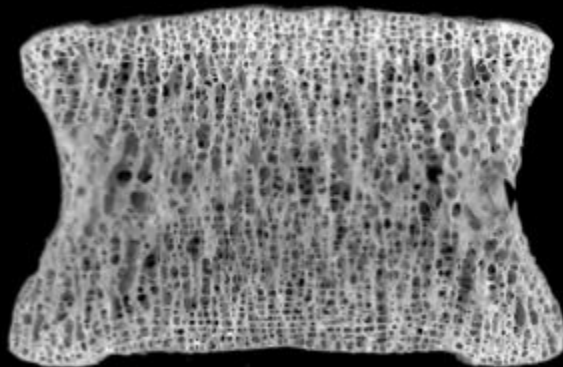
- Osteoporosis
- Osteoporosis Imaging
- Trabecular Plate Rod Microarchitecture
- Bone Measures using Multi-row Detector CT Imaging
- Results from Human Studies

Overview

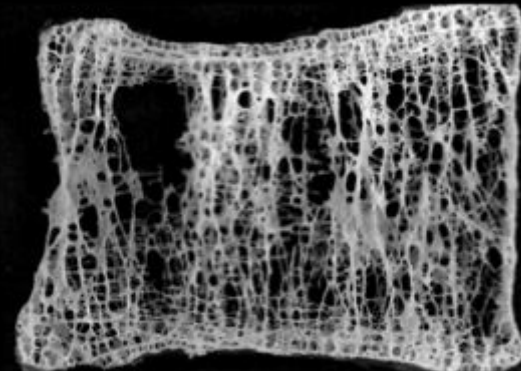
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Osteoporosis

- The word osteoporosis literally means “porous bones”
- Over time, osteoporosis reduces bone mass and degenerates bone structure, and therefore bone strength is decreased
- Thus, bone becomes fragile and easy to break
- For someone with severe osteoporosis, even a sudden movement may cause bone fracture



Normal bone in vertebrae



Same bone location in a osteoporosis patient

<http://www.bonedisease.info/disease/osteoporosis/which-bone-affected-by-osteoporosis-the-most/>

Osteoporosis and Fractures

- Osteoporosis affects nearly half of the men and women over the age of 75
- About 44 million people in the United States are at risk for osteoporosis causing 1.5 million fragility fractures annually
- Nearly, 40% of women and 13% of men suffer a fragility fracture in their lifetimes
- The estimated number of hip fractures worldwide will rise from 1.66 million in 1990 to 6.26 million in 2050
- Major osteoporosis fractures occur at hip, spine and forearm
- Osteoporotic hip fractures are especially devastating, reducing life expectancy by 10-20%
- More than three-quarters of all hip fractures occur in women



Major fracture sites

http://www.vidasaludynegocios.com/index.php?dispatch=products.view&product_id=30529

Treatments

- Treatment includes medication, healthy diet, and weight-bearing exercise to help prevent bone loss and strengthen already weak bones
- Self-care
 - ✓ Healthy diet
 - ✓ Physical exercise
 - ✓ Stop smoking
- Medications
 - ✓ Vitamin
 - ✓ Dietary supplement
 - ✓ Antacid
 - ✓ Bone health
 - ✓ Hormone

Treatments

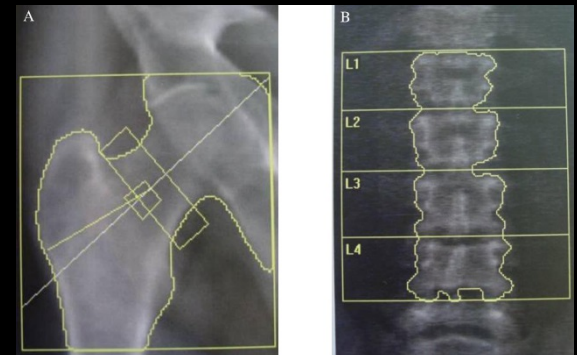
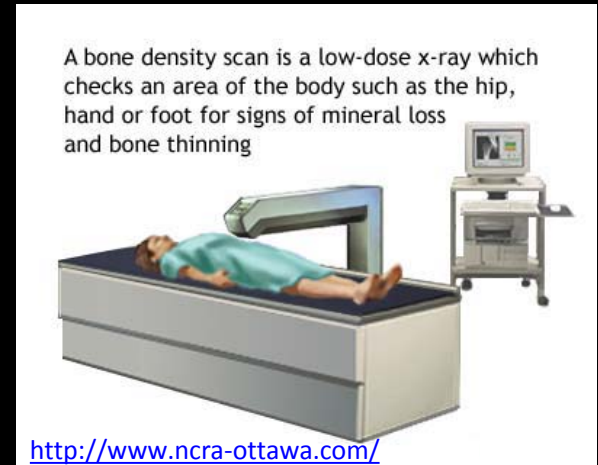
- Treatment includes medication, healthy diet, and weight-bearing exercise to help prevent bone loss and strengthen already weak bones
 - Self-care
 - ✓ Healthy diet
 - ✓ Physical exercise
 - ✓ Stop smoking
 - Medications
 - ✓ Vitamin
 - ✓ Dietary supplement
 - ✓ Antacid
 - ✓ **Bone health**
 - ✓ **Hormone**
- Therapeutic treatments for osteoporosis are expensive with associated side effects
 - Accurate assessment of fracture risk, and clear guidelines to initiate preventive interventions and monitor treatment response, are urgent needs in public health
 - **Osteoporotic imaging** plays a central role in that process

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Dual-Energy X-Ray Absorptiometry (DXA)

- At present, dual-energy X-ray absorptiometry (DXA) measured areal BMD is used to diagnose osteoporosis
- DXA measures of whole body, hip and spine are popularly used
- Being an areal 2-D measure, DXA has several limitations
 - ✓ sensitivity to bone size, thus overestimating fracture risk in individuals with small body size
 - ✓ lack of accuracy in the setting of degenerative changes in the hip and spine
- It is known that the majority of individuals who suffer fragility fractures are misclassified by DXA as not having osteoporosis, i.e., their T-scores are actually > -2.5



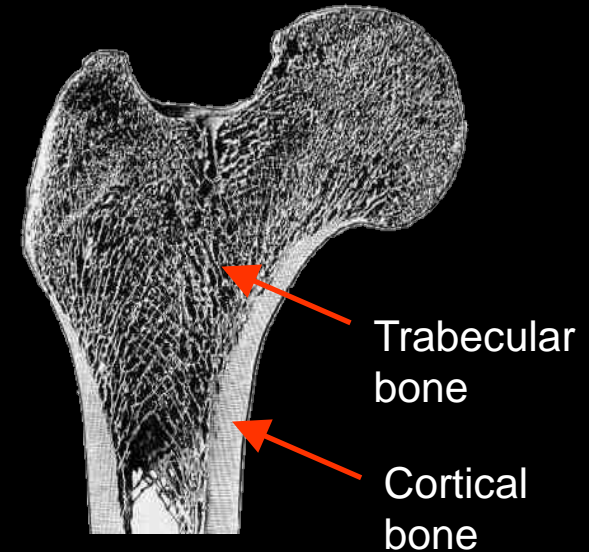
DEXA assessment of BMD of the femoral neck (A) and the lumbar spine (B)

https://en.wikipedia.org/wiki/Dual-energy_X-ray_absorptiometry

Osteoporosis and Bone Structure

There are two types of bone

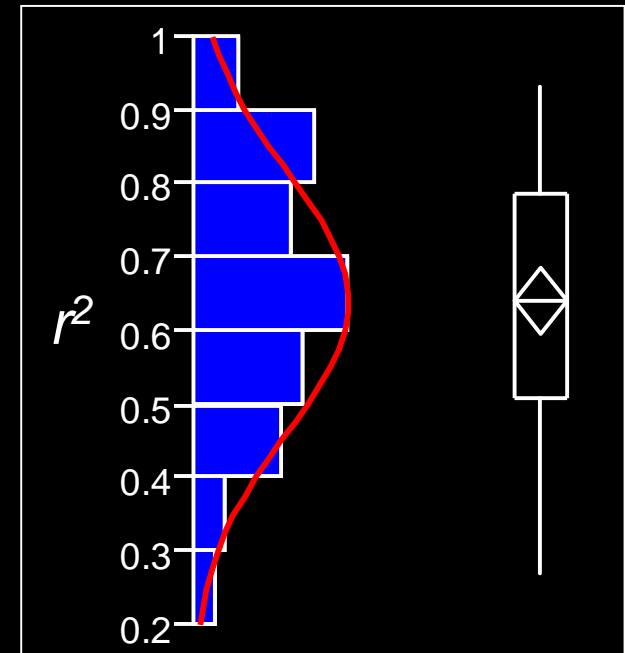
- Cortical bone (**Cb**) is the hard outer layer of the bone
- Trabecular bone (**Tb**) is the sponge-like internal structure of the bone
- Cb is denser, stronger, and stiffer for more strenuous activities
- Cb can sustain greater stress but less strain before failure
- Tb can sustain larger strains before failing
- Tb has a greater capacity to store energy since it is porous and filled with fluid
- Osteoporosis can lead to thinning of both types of bone which makes bones more susceptible to breaks



Bone Mineral Density and Mechanics

How Predictive is bone mineral density (BMD) of the Bone's Mechanical Behavior?

- Meta analysis
- N=38 (1985-2000)
- Various parameters of “strength”
- Mean $r^2 = 0.64 \pm 0.17$

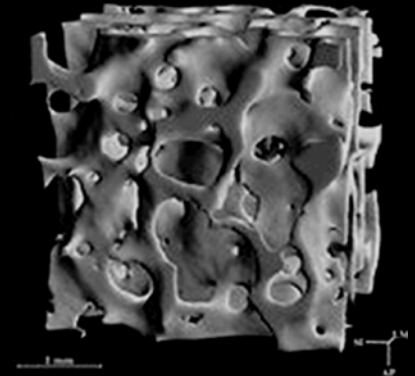


BMD only accounts for approximately 60 to 70% of the variability in bone strength

Bone Mineral Density and Structure

- Although osteoporosis is defined by low BMD, BMD explains 60-70% of the variability in bone strength
- The remaining variability due to the cumulative and synergistic effects of other factors, including geometry and micro-architecture of Cb and Tb
- Several clinical studies have reported that cortical bone thinning and high porosity is associated with increased risk of osteoporotic low-trauma fractures
- A large number of histologic studies have confirmed the relationship between erosion of trabeculae from plates to rods and fracture risk
- Reduced trabecular connectivity are observed in patients with vertebral crush fractures
- There is evidence suggesting that reduced transverse trabeculae are associated with decreased bone strength leading to failure due to buckling of longitudinal trabeculae

Normal



Osteoporosis

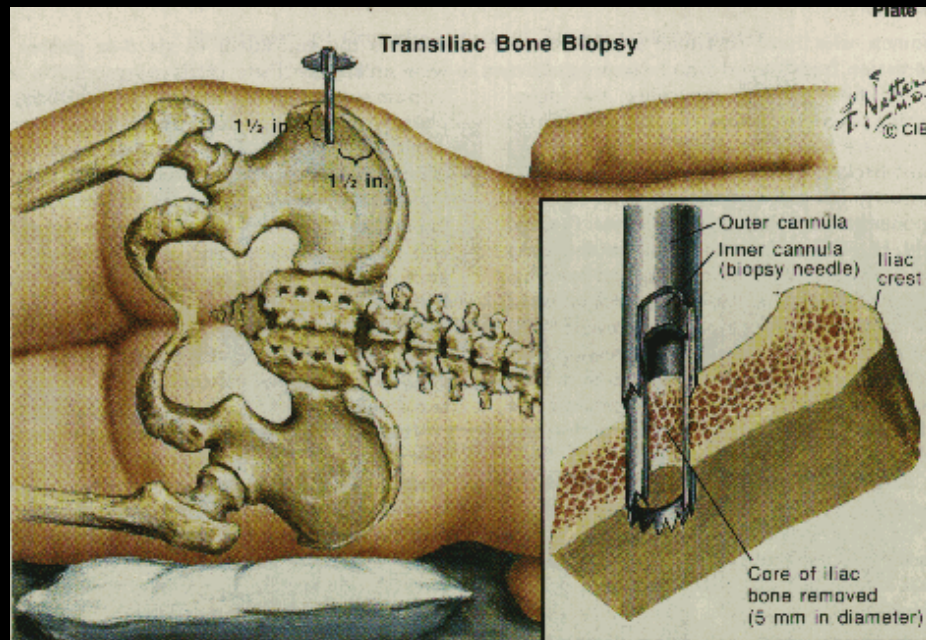


Hildebrand et al, JBMR, 1999

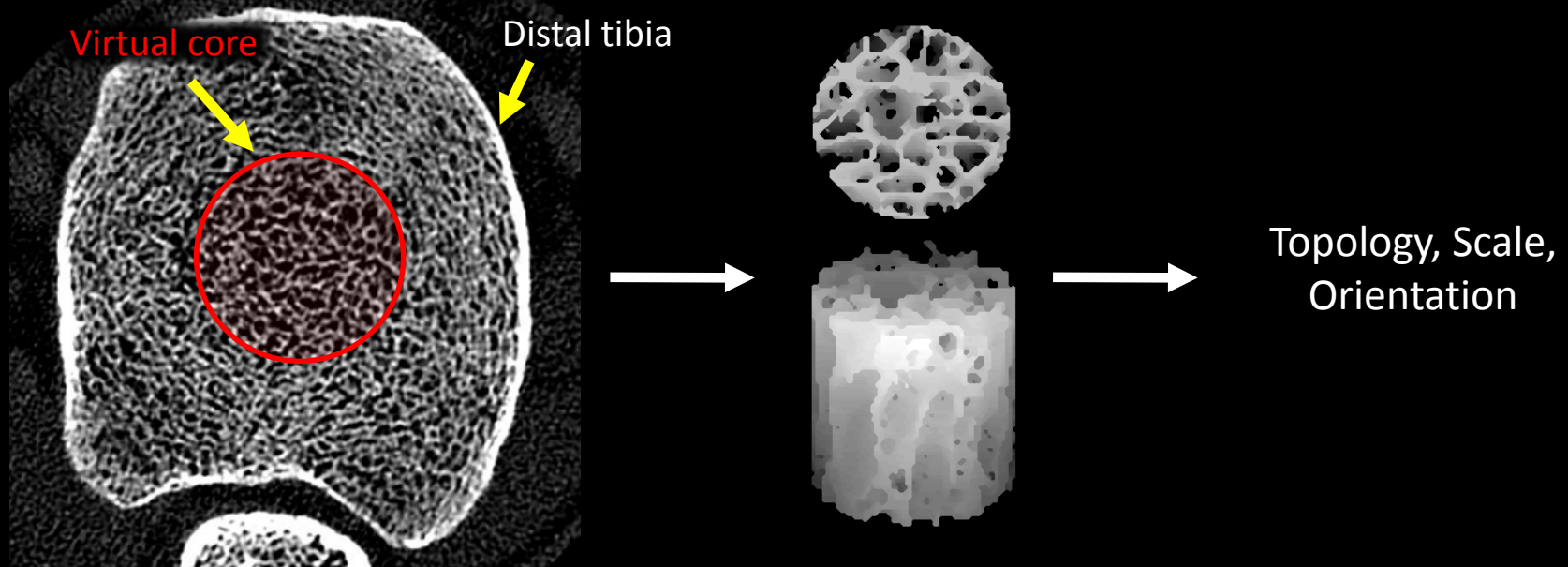
Bone Biopsy

Quantifying Architecture via Bone Biopsy

- Iliac crest or rib
- Painful, risky, and limited retests
- Not suitable for controls or time-series analysis



In Vivo Imaging Offers an Opportunity for Virtual Bone Biopsy



Features

- Analogous to bone biopsy
- Virtual core is isolated from 3D image data sets.
- Core is subjected to analysis

Challenges

- Reduced resolution
- Limited signal-to-noise ratio

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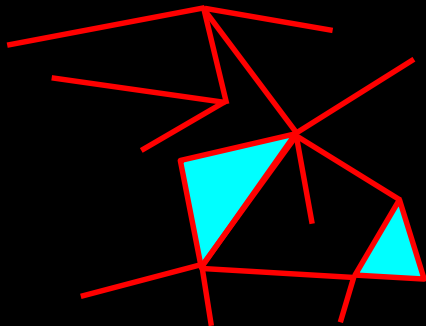
Topology of Trabecular Networks

Topological analysis of line skeletonized structure

3D Euler Poincaré Formula:

$$\chi = \text{objects} - \text{tunnels} + \text{cavities} \\ = \text{nodes} - \text{edges} + \text{faces}$$

$$\text{Connectivity Index} = 1 - \chi$$



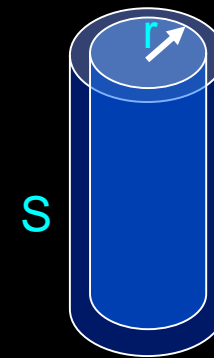
objects: 1
 # tunnels: 1
 # cavities: 0

 # nodes: 17
 # edges: 19
 # faces: 2

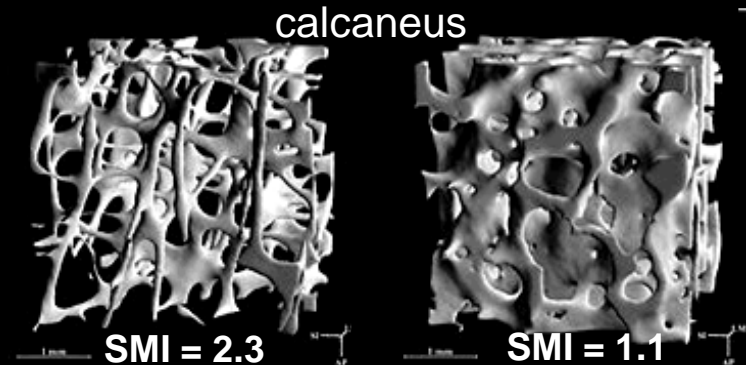
$$\chi = 0$$

Structure-Model Index (SMI)

$$\text{SMI} \propto \left(\frac{\partial S}{\partial r} \right)$$



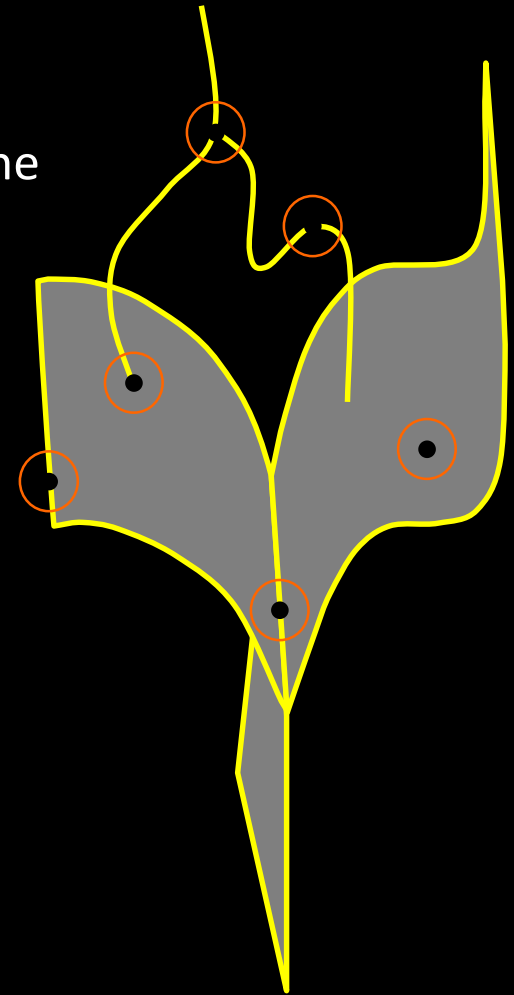
SMI=relative change in surface area (S) upon radial (r) expansion



Hildebrand et al, J Bone Miner Res, 1999

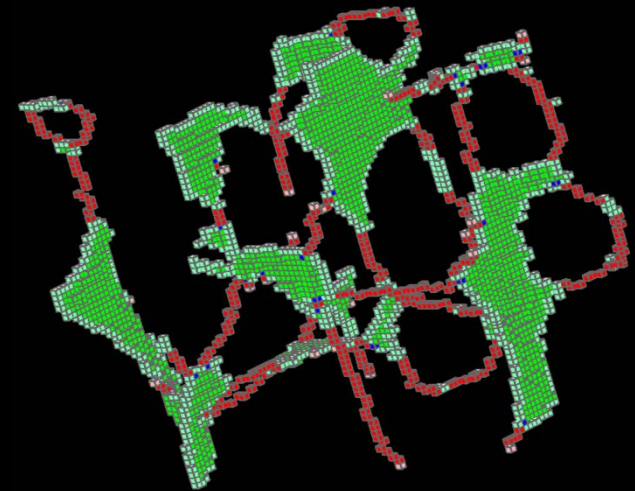
Trabecular Plate-Rod Characterization using Digital Topological Analysis

- Topological class (curve, surface junctions) at any location may be unambiguously determined from the topological numbers (#objects (ξ), #tunnels (η), and #cavities (δ))
- Edge: $\xi = 1$; $\eta = 0$; $\delta = 0$
- Curve Interior: $\xi = 2$; $\eta = 0$; $\delta = 0$
- Surface Interior: $\xi = 1$; $\eta = 1$; $\delta = 0$
- Curve-Curve junction: $\xi > 2$; $\eta = 0$; $\delta = 0$
- Surface-Curve junction: $\xi > 1$; $\eta = 1$; $\delta = 0$
- Surface-Surface junction: $\xi = 1$; $\eta > 1$; $\delta = 0$



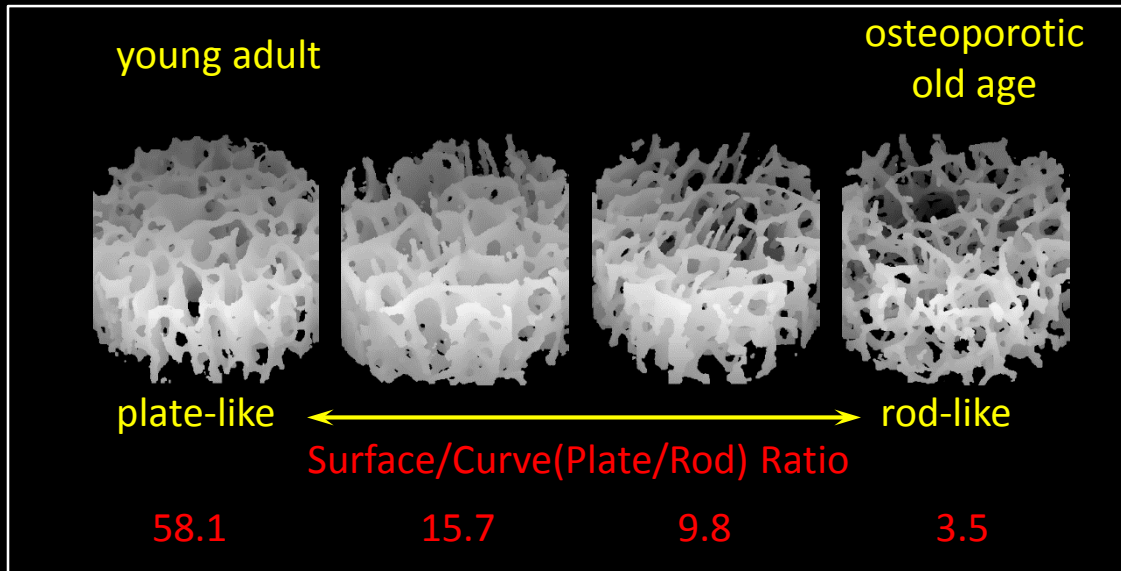
Digital Topological Analysis

- Identifies plates/rods and other topological entities
- Able to distinguish between fracture/ non-fracture groups via *in vivo* MRI
- Being used by several leading research groups

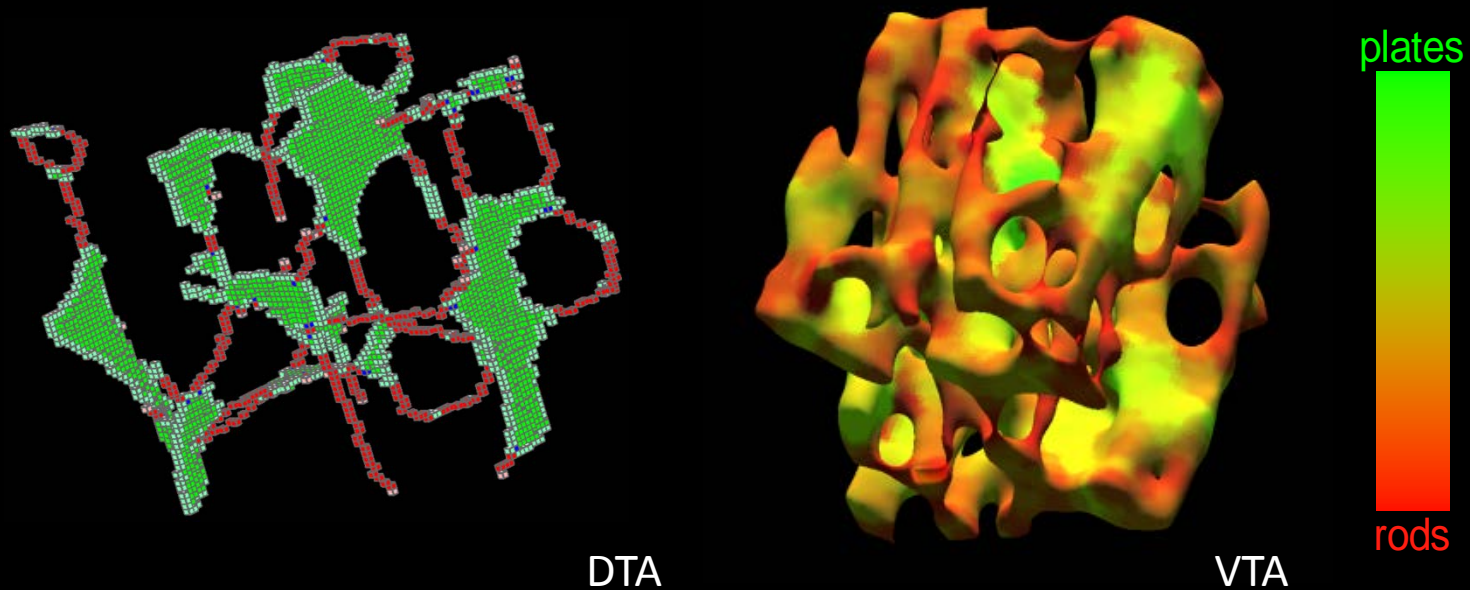


Surface = plate
Rod = curve
Junction

Age and disease-related
topological changes

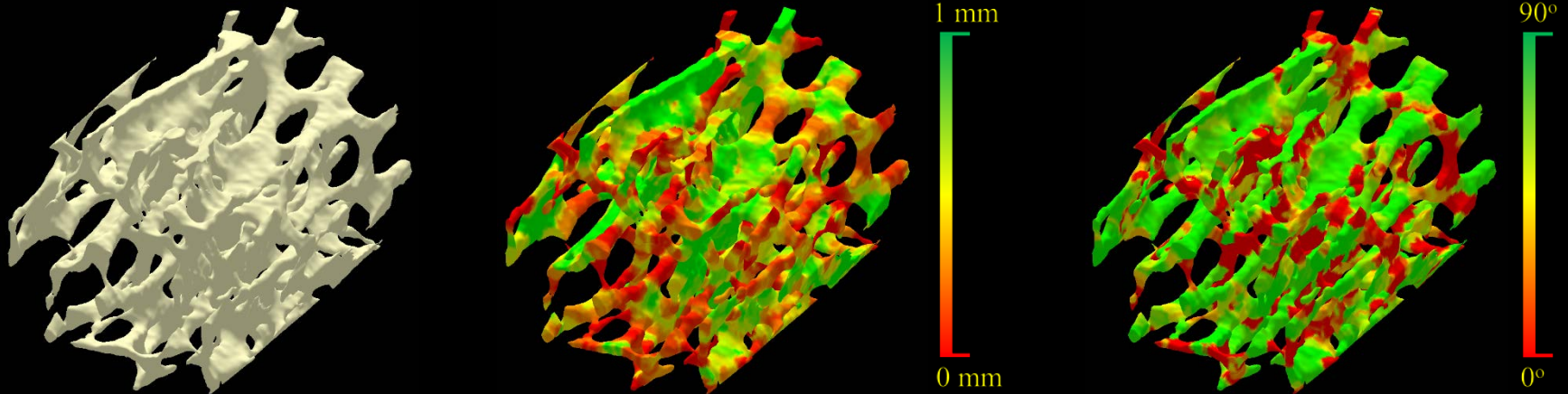


Volumetric Topological Analysis



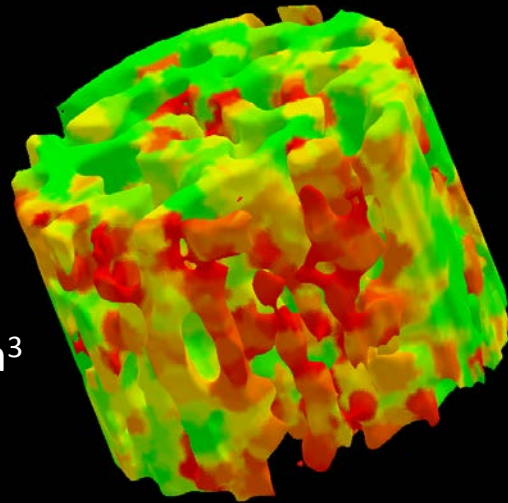
- Quantify trabecular bone architecture at *in vivo* resolution
 - Plateness and rodness on the continuum between perfect plates and perfect rods
 - More accurately captures gradual conversion from Tb plates to rods at the level of individual trabeculae

Tensor Scale Analysis

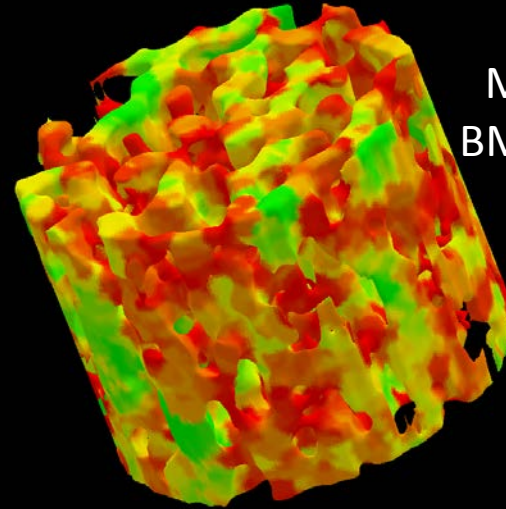


- Quantify trabecular bone architecture at *in vivo* resolution
 - Plateness and rodness on the continuum between perfect plates and perfect rods
 - Local trabecular orientation classifying longitudinal (vertical) and transverse (horizontal) structures

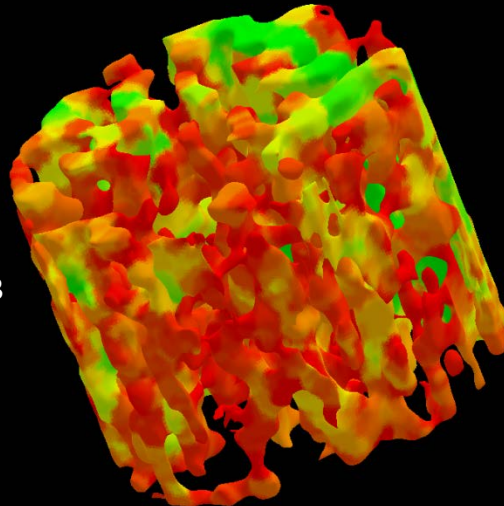
Trabecular Plate-Rod Measures and Bone Strengths



Modulus: 3.3 GPa
BMD: 1.31 gm/cm³
Tb.PW : 464 μm
Tb.PR: 0.58



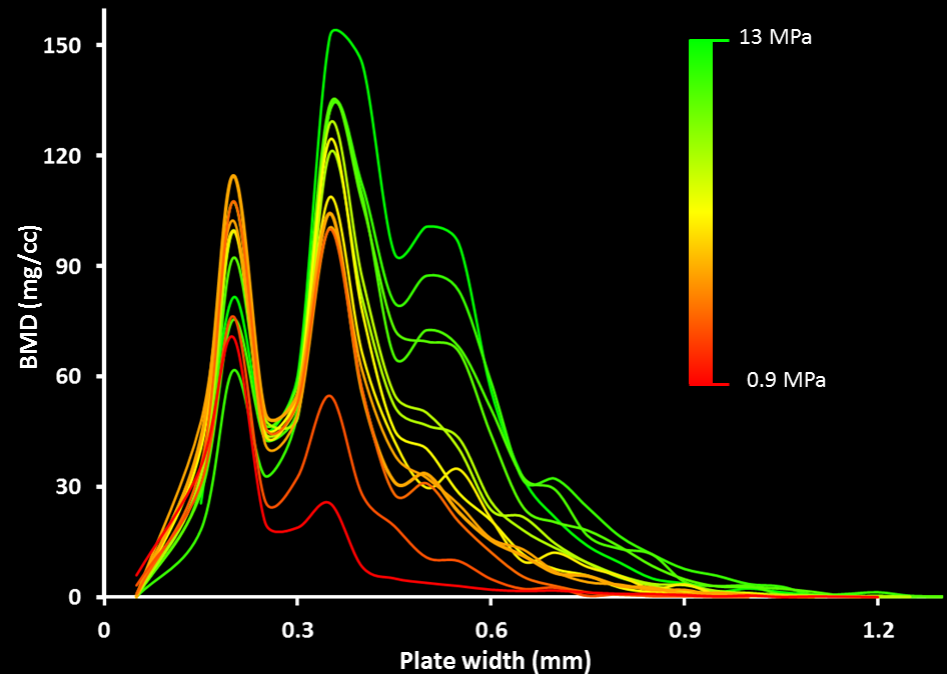
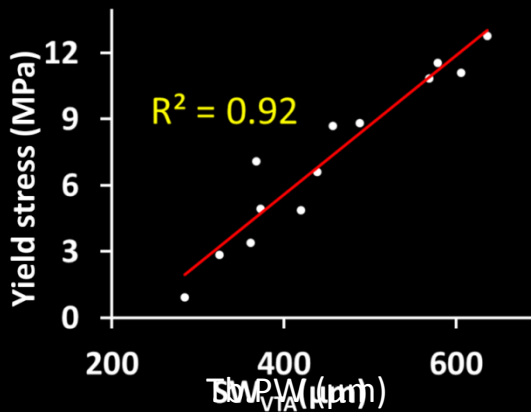
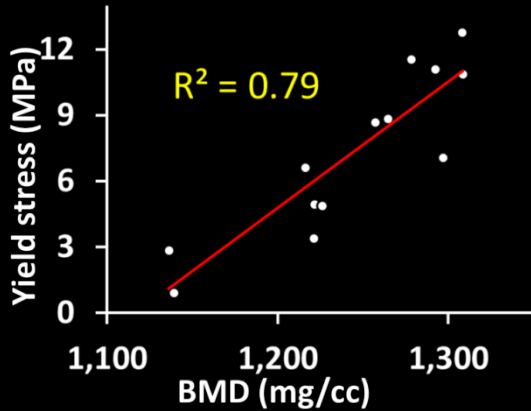
Modulus: 2.2 GPa
BMD: 1.27 gm/cm³
Tb.PW: 385 μm
Tb.PR: 0.38



Modulus: 1.5 GPa
BMD: 1.20 gm/cm³
Tb.PW: 340 μm
Tb.PR: 0.26

8% reduction in BMD
reduced bone strength to
half and manifest a 50%
alteration in micro-
architecture

Ability To Predict Mechanical Properties

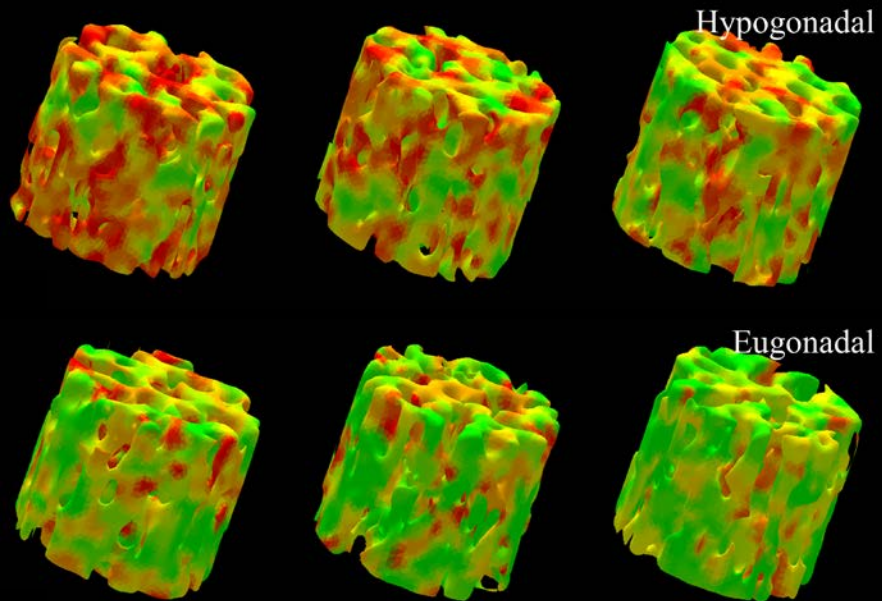


High predictability of experimental biomechanical properties.

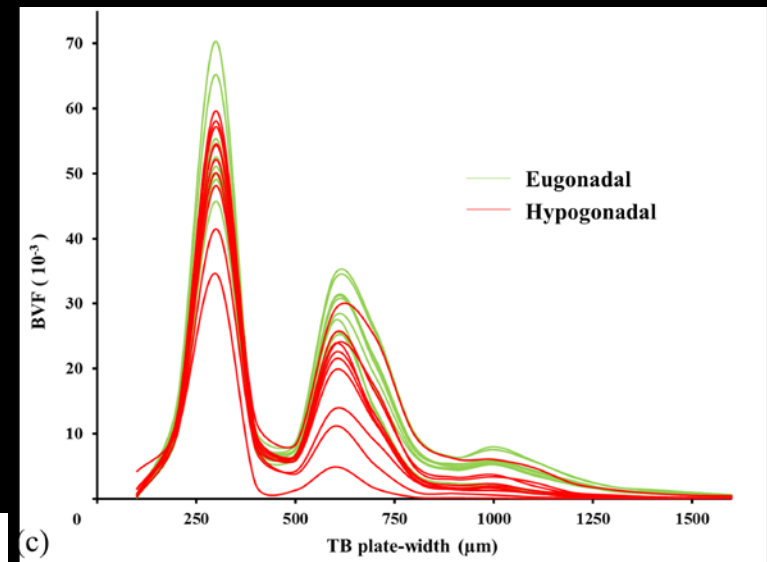
Bone mass distribution at different plate width: a new class of information

Bone Micro-Architecture among Eugonadal and Hypogonadal Men

$N = 20$ MRI Study (age and race-matched)



Trabecular bone plate-rod micro-architecture among hypogonadal and eugonadal men

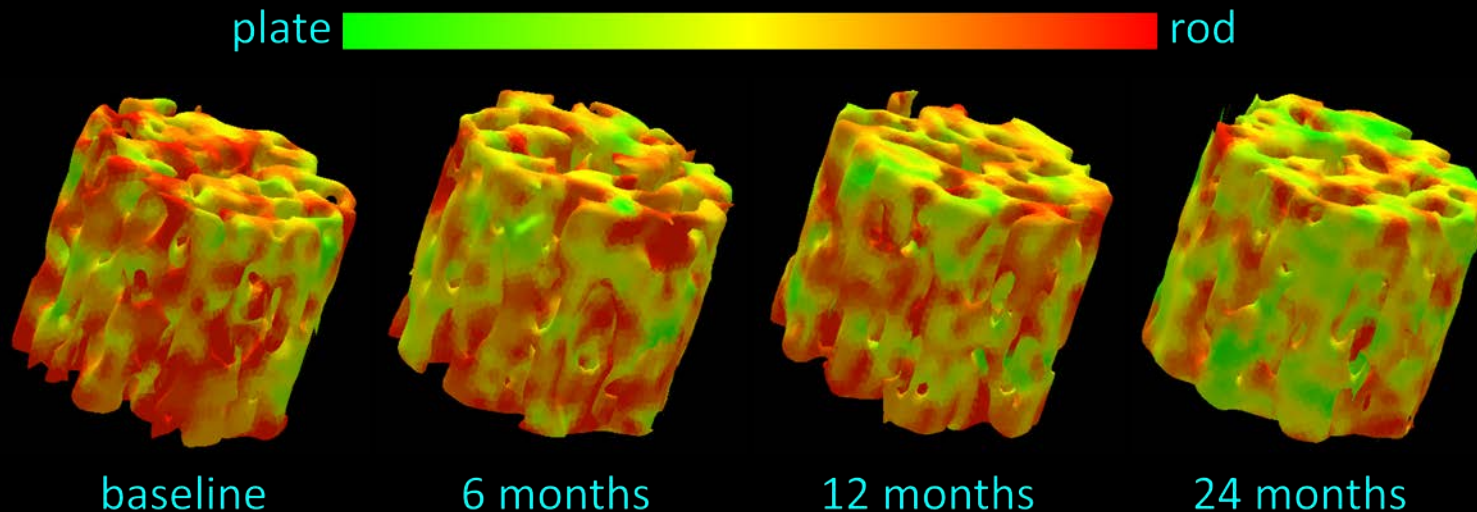


Bone mass distribution at different plate width: a new class of information

- 44 % ($p = 0.001$) greater Tb plates in eugonadal men than hypogonadal men
- No significant difference in rod volume

Treatment Effects Hypogonadal Men

$N = 10$ Two year follow-up MRI study



Treatment effects in trabecular bone plate-rod micro-architecture in hypogonadal men

- 6.5 % ($p = 0.06$) increase in trabecular bone plate volume after 6 months
- 16.2 % ($p = 0.003$) increase in trabecular bone plate volume after 24 months
- No significant difference in rod volume even after 24 months of treatment

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Major Advantages of Modern MDCT Scanners

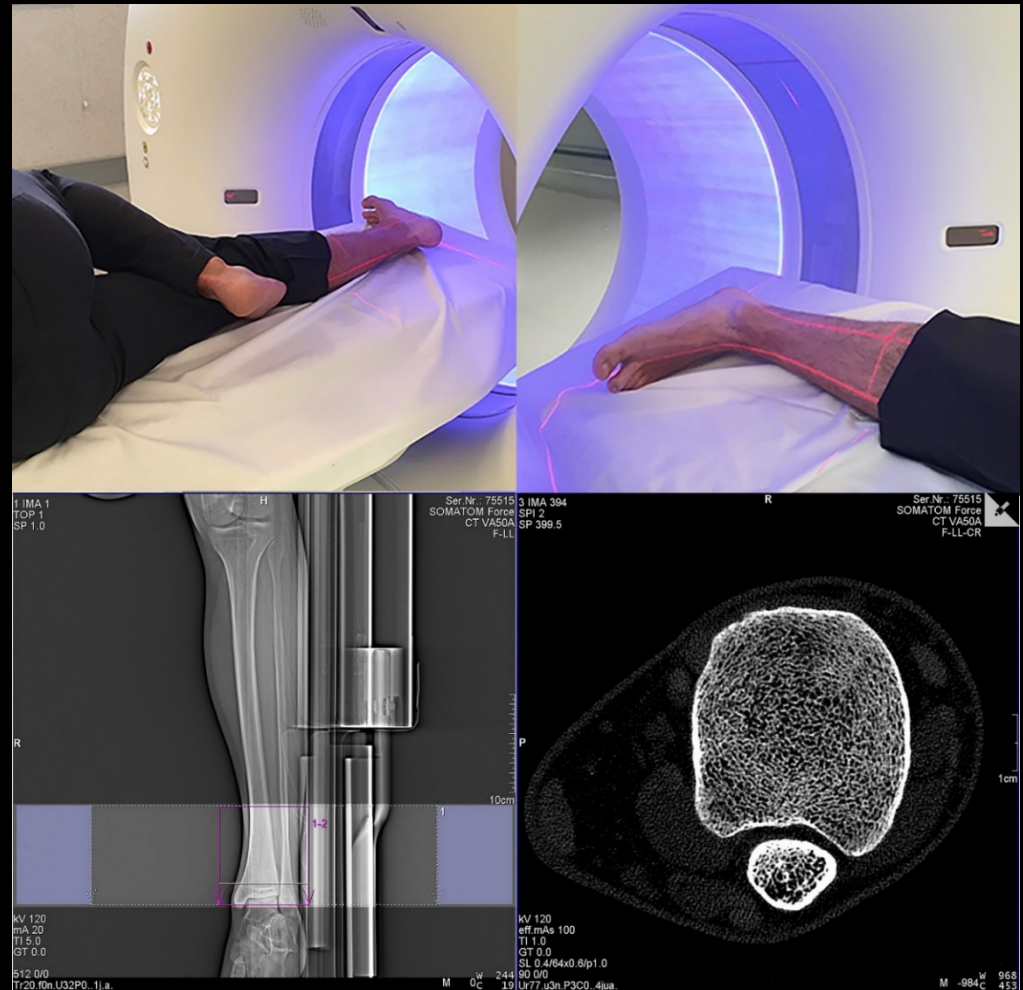
- **High spatial resolution:** State-of-the-art CT scanners provide high spatial resolution allowing segmentation and quantitative assessment of TB micro-architecture
 - ✓ The Siemens Force scanner achieves 167 μm (10% MTF) in-plane resolution and 282 μm (10% MTF) z-plane resolution
- **Ultra-high speed scanning:** Modern CT scanners are capable of acquiring a 10 cm scan-length at a peripheral site using an UHR mode in just 6.8 sec
- **Ultra-low radiation:** Modern MDCT scanners allow high resolution Tb imaging at less than 50 μSv radiation dose
- **Large scan-length:** Useful for automatic selection of anatomically consistent regions-of-interest (ROIs)
 - ✓ Positioning error is a serious challenge for HR-pQCT
 - ✓ A positioning error by 0.5 mm may result in a 2% error in bone measures at the distal tibia

MDCT Scan Protocol

- Single X-ray source spiral acquisition at 120 kV, 100 effective mAs, 1sec rotation speed, pitch factor: 1.0
- Number of detector rows: 64
- Scan time: 5.8 seconds, collimation: 64× 0.6 mm
- Total effective dose equivalent: 50 μ Sv \approx 5 days of environmental radiation in the United States
- Siemens z-UHR scan mode is applied enabling Siemens double z sampling technology
- Images are reconstructed at 400 μ m slice-thickness with 200 μ m slice-spacing and 150 μ m pixel-size using Siemens's special kernel Ur77u with Edge Technology to achieve high spatial resolution

In Vivo MDCT Scan Setup

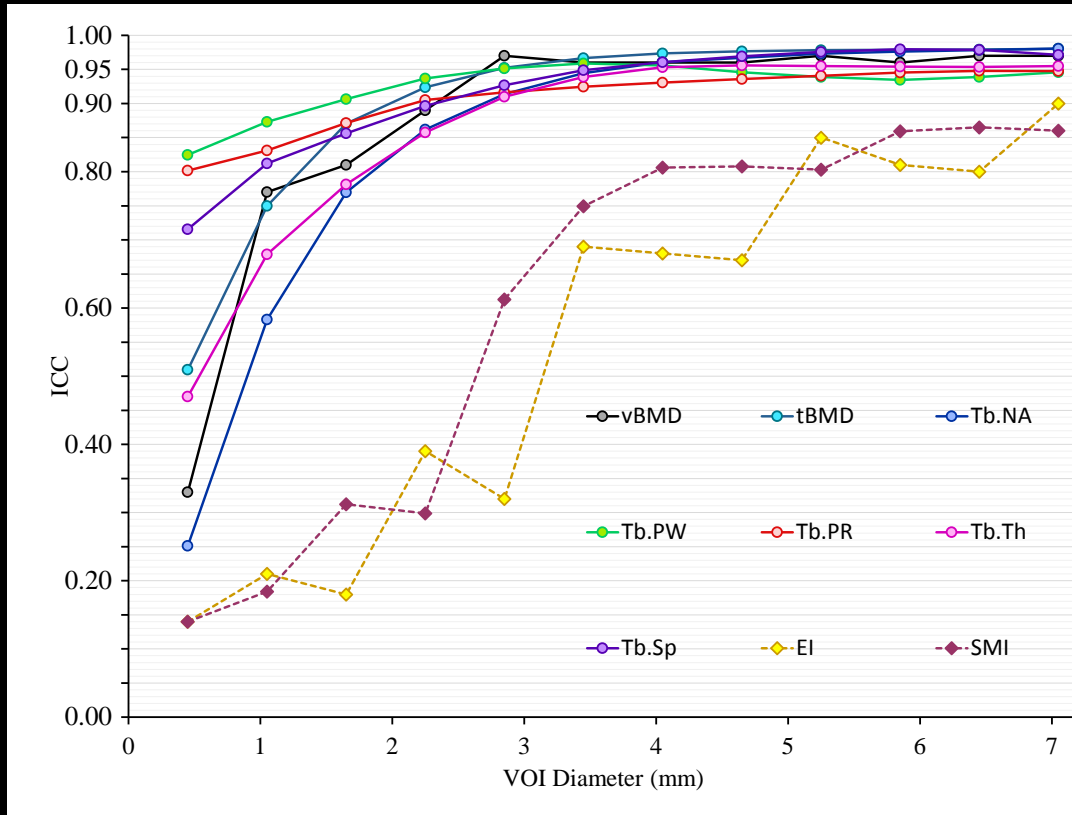
- Laser beam projections are used to align the tibial long axis with the central z axis of the scanner
- This alignment step is important to achieve the highest image resolution and to standardize trabecular bone measures
- The distal tibial end-plateau is included in the FOV used as reference to determine different tibial locations for ROI selection



The List of MDCT Derived Tb Measures

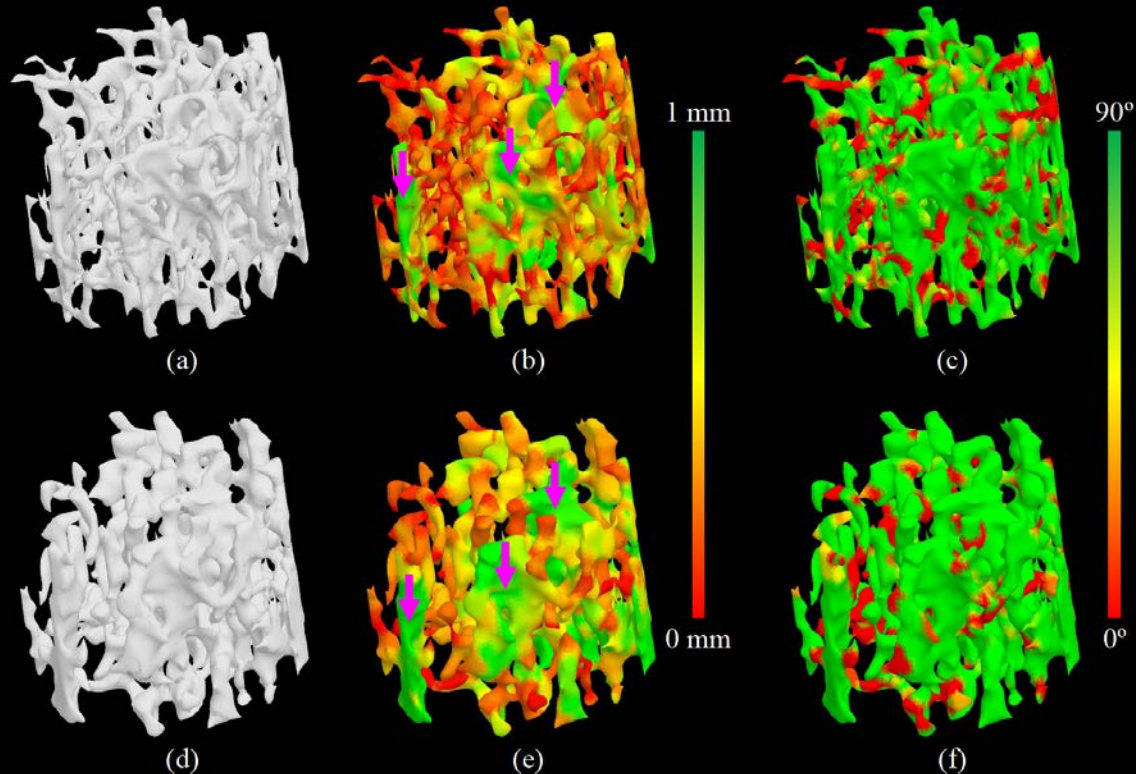
<i>Parameter (unit)</i>	<i>Description</i>
vBMD (mg/cm ³)	Volumetric trabecular bone mineral density
tBMD (mg/cm ³)	Volumetric trabecular bone mineral density contributed by transverse trabeculae characterized by tensor scale analysis
Tb.NA (cm ² /cm ³)	Trabecular bone network area density, i.e., the average area of the medial surface of segmented bone per unit VOI
Tb.PW (μm)	Mean trabecular plate-width computed by tensor scale analysis
Tb.PR (no unit)	Ratio of total plateness and rodness counts over a VOI computed by tensor scale analysis
Tb.Th (μm)	Mean trabecular thickness computed by star-line analysis
Tb.Sp (μm)	Mean trabecular separation, i.e., the space between trabecular structures computed by star-line analysis
EI (no unit)	Erosion index—a summary measure of digital topological analysis of TB aimed to represent the extent of bone erosion
SMI (no unit)	An indicator of the structure of trabeculae; SMI is '0' for parallel plates and '3' for cylindrical rods

Repeatability of MDCT Tb Measures



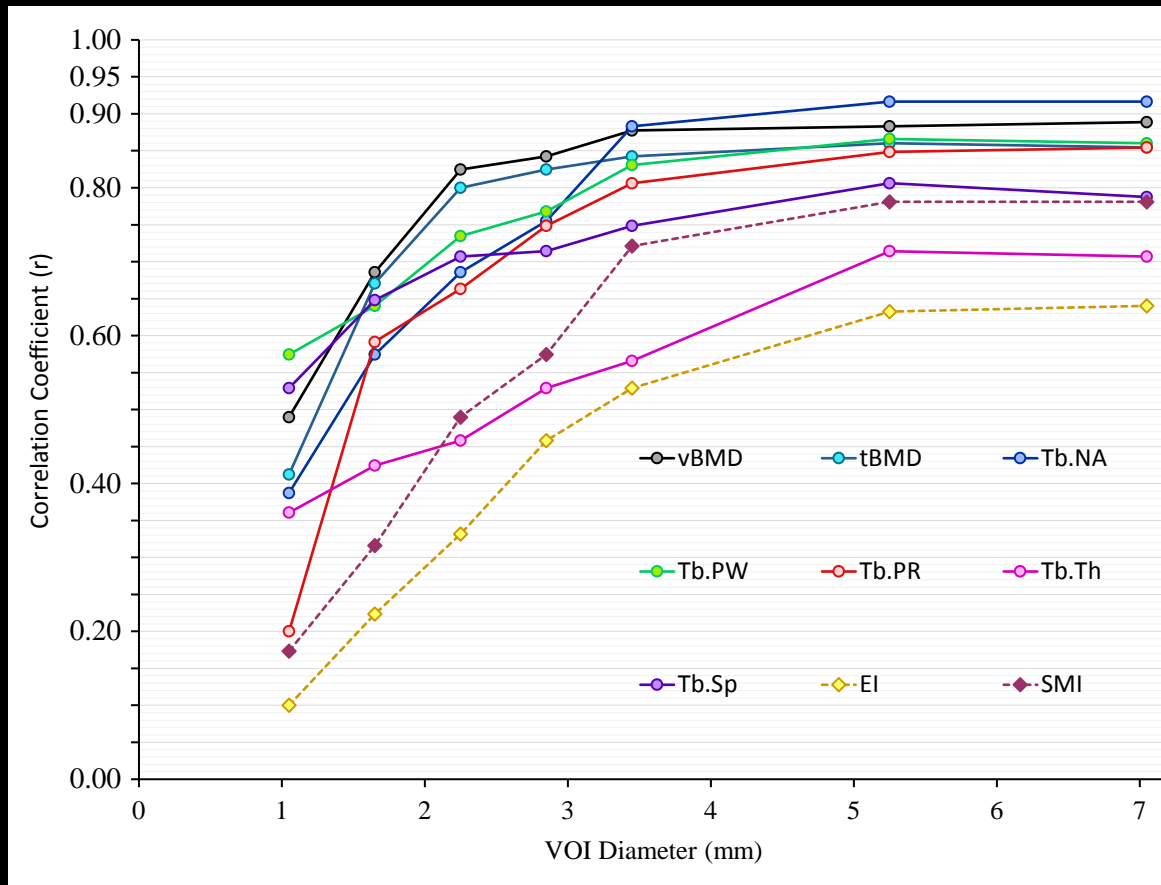
Repeat scan reproducibility of Tb measures on an MDCT scanner using cadaveric ankle specimens (n = 25)

Validation of MDCT Tb Measures



- Tb plate-rod and orientation characterization using micro-CT (top row) and MDCT scanners (bottom row)
- Although, the effects of resolution difference between the two scanners are apparent, regional agreement of microstructural characterization is notable

Validation of MDCT Tb Measures



Correlation analysis of the values of Tb measures derived from micro-CT and MDCT imaging of cadaveric ankle specimens (n = 25)

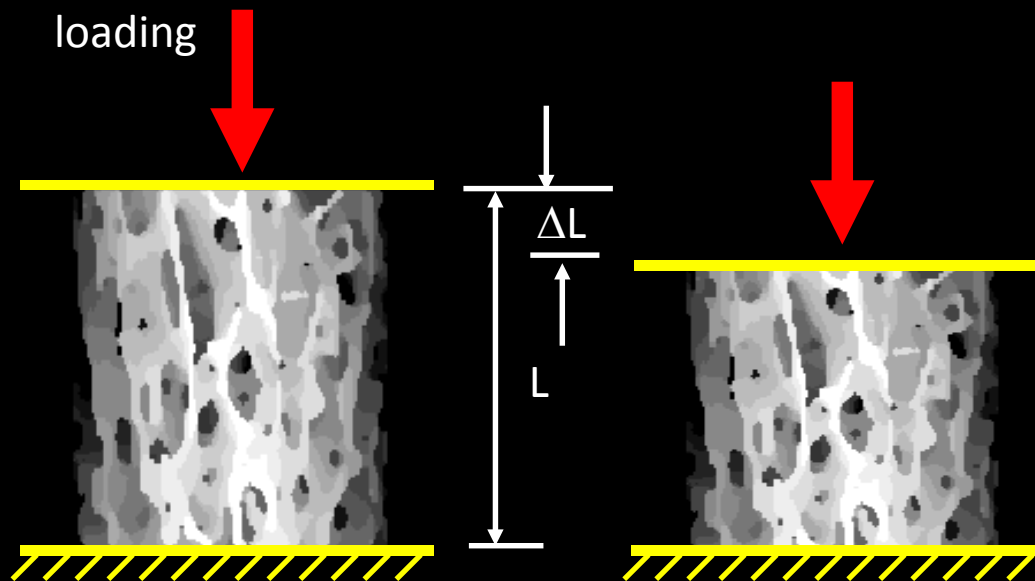
Validation of MDCT Tb Measures

TB measure	Correlation Coefficients (r)	micro-CT (mean value)	MDCT (mean value)
vBMD (mg/cm ³)	0.88	1158	993
tBMD (mg/cm ³)	0.86	194	120
Tb.NA (cm ² /cm ³)	0.92	0.10	0.07
Tb.PW (μm)	0.87	541	861
Tb.PR (no unit)	0.85	2.85	7.02
Tb.Th (μm)	0.71	133	160
Tb.Sp (μm)	0.81	348	468
EI (no unit)	0.63	0.20	0.67
SMI (no unit)	0.78	0.76	2.23

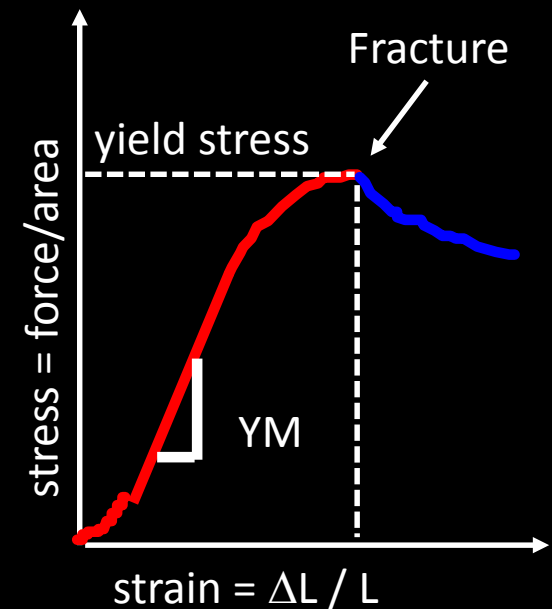
Correlation and mean values of Tb measures derived from micro-CT and MDCT imaging of cadaveric ankle specimens at VOI size of 5.25 mm (n = 25)

Ability of MDCT Tb Measures to Predict Mechanical Properties

Measuring Elastic Properties



Strains were recorded using an extensometer reading



Young's Modulus (YM)
= slope

Ability of MDCT Tb Measures to Predict Mechanical Properties

Pearson correlation coefficient (r)

TB measure	MDCT bone measures versus bone strength		micro-CT bone measures versus bone strength	
	Yield stress	Young's modulus	Yield stress	Young's modulus
vBMD (mg/cm ³)	0.785	0.698	0.763	0.738
tBMD (mg/cm ³)	0.861	0.813	0.872	0.791
Tb.NA (cm ² /cm ³)	0.855	0.712	0.838	0.807
Tb.PW (μm)	0.893	0.757	0.902	0.802
Tb.PR (no unit)	0.838	0.722	0.854	0.820
Tb.Th (μm)	0.849	0.765	0.817	0.685
Tb.Sp (μm)	0.851	0.730	0.848	0.764
EI (no unit)	0.780	0.536	0.781	0.670
SMI (no unit)	0.786	0.541	0.821	0.743

Correlation of different MDCT and micro-CT TB measures with yield stress and Young's modulus of TB cores from cadaveric ankle specimens determined by mechanical testing (n = 25)

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Study 1

Aim: To determine whether MDCT bone data from multiple scanners can be used in large multi-site or longitudinal studies

Data-Continuity for Tb Measures from Two MDCT Scanners (n = 20)

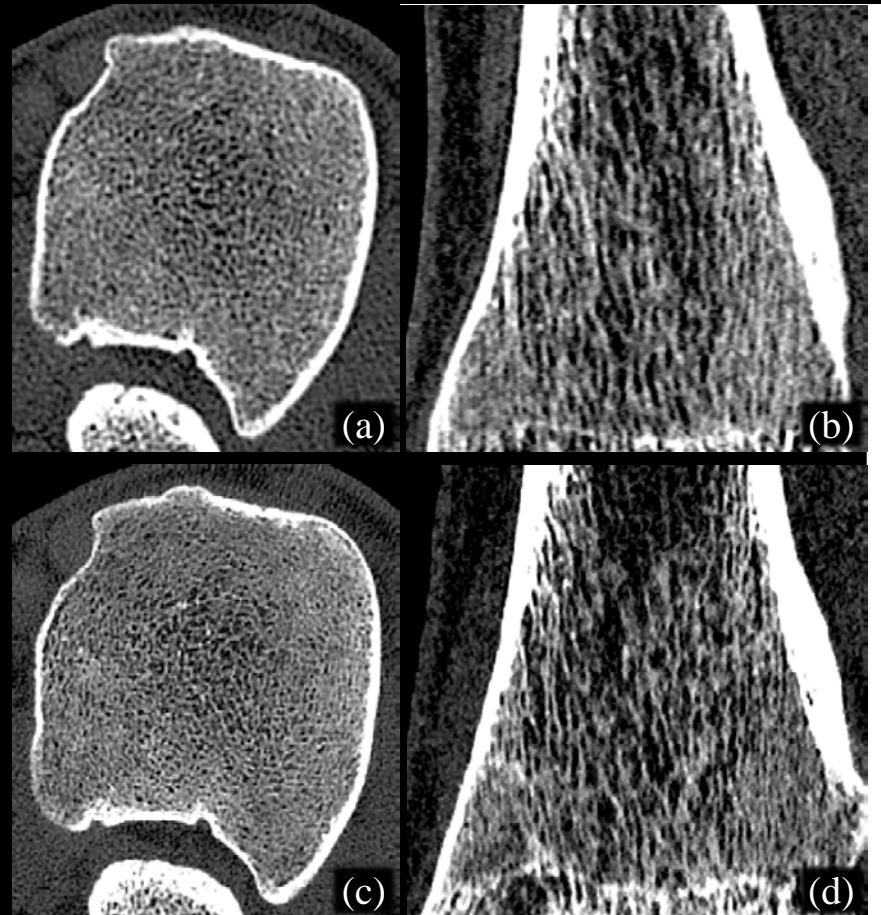
- A pertinent challenge with MDCT for bone research emerges due to wide variation in imaging and reconstruction features from different vendors and rapid upgrades in technology
- This raises concerns of data uniformity in large-scale multi-site or longitudinal studies that typically involve data from multiple scanners
- the distal tibia of twenty volunteers (age: 26.2 ± 4.5 Y, 10 female) was scanned using the **Siemens SOMATOM Definition Flash** and the higher resolution **Siemens SOMATOM Force** scanners with an average 45-day time gap between scans.

10% MTF (lp/cm)

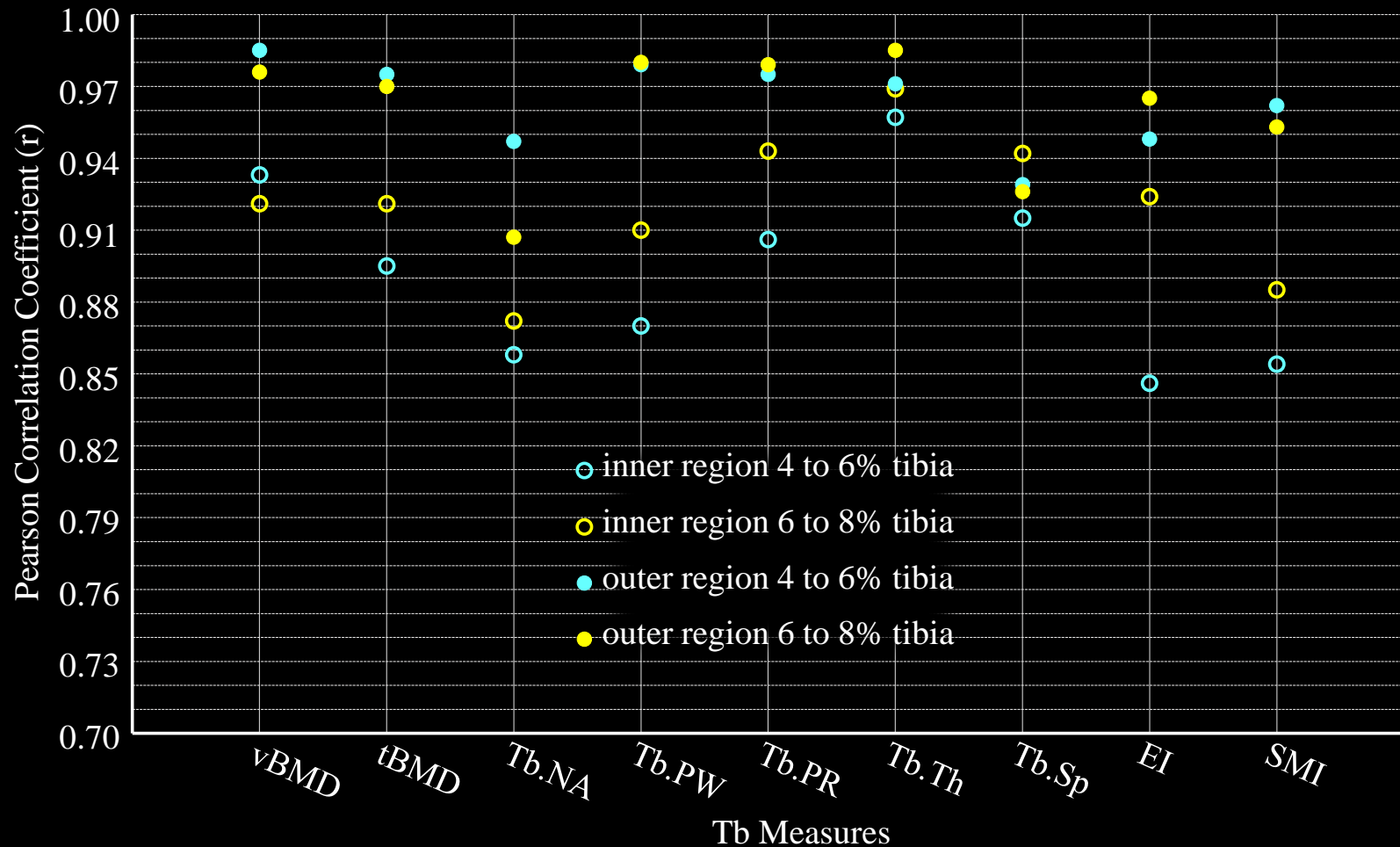
Scanner	Kernel	CT parameters	xy-plane	z-direction
Siemens Flash	U70u	120 kV, 200mAs, pitch : 1	16.2	17.9
Siemens Force	Ur77u	120 kV, 100 mAs, pitch : 1	24.8	21.0

Resolution Effects for Two MDCT Scanners

MDCT images of the lower portion of the left leg of a healthy volunteer scanned using the Siemens Flash (low resolution) (upper row) and Force (high resolution) (lower row) scanners



Correlation for Tb measures obtained from the Two Siemens Flash scanners



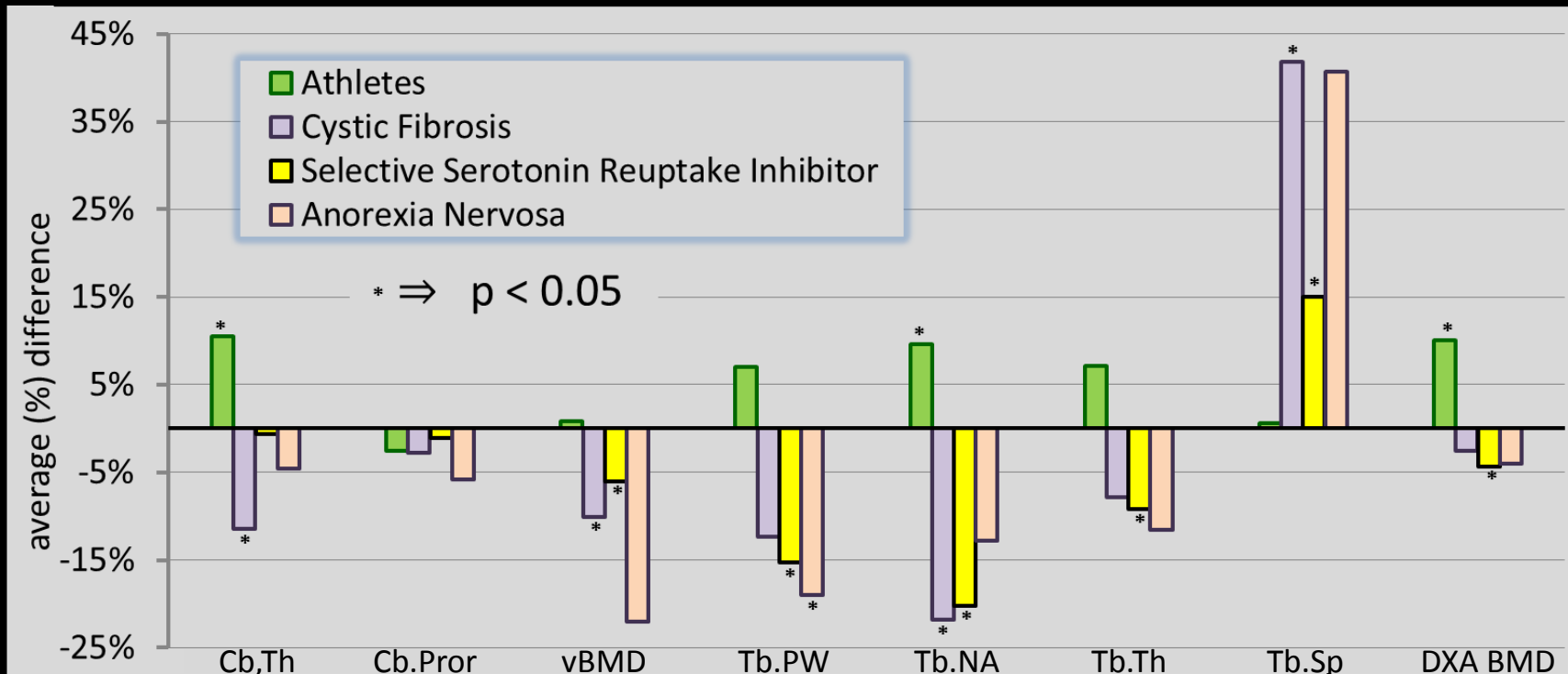
Discussion

- Tb micro-architectural measures estimated from the two different MDCT scanners possess high linear correlation ($r > 0.9$)
- Higher correlations of Tb measures from the two scanners were observed for the outer region at both the 4-6 % and 6-8% distal tibia
- *In vivo* measures of TB micro-architecture from two scanners can be used in a cross-sectional or longitudinal study after adjustments using calibration equations, if needed. The calibration equations will be useful in multi-center studies to distinguish whether an observed difference in a parameter is associated with scanner differences or “real” difference between measured bones
- A non-significant interaction effect for distal tibial location of TB measures and slope showed that, for a TB measure, similar calibration is required independently of the location used for measurement
- All measures with lower CCCs would require some kind of calibration.

Study 2

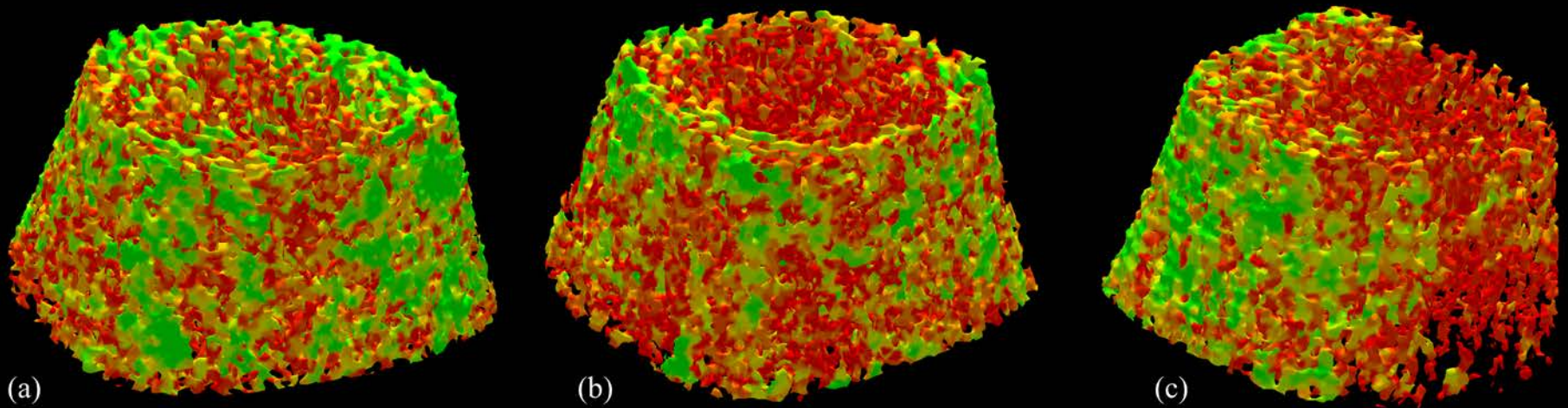
Aim: To determine differences in bone structures in different human study groups

Results of a Human Pilot Study



Average differences of bone measures in athlete (N=10), cystic fibrosis (N=11), selective serotonin reuptake inhibitor (N=12), and anorexia nervosa (N=4) groups as compared to age-sex-BMI-similar healthy controls from the Iowa Bone Development Study (N=102). Age-sex-height matching was used for the anorexia nervosa group.

Bone Characterization in Different Patient Groups



(a)

(b)

(c)

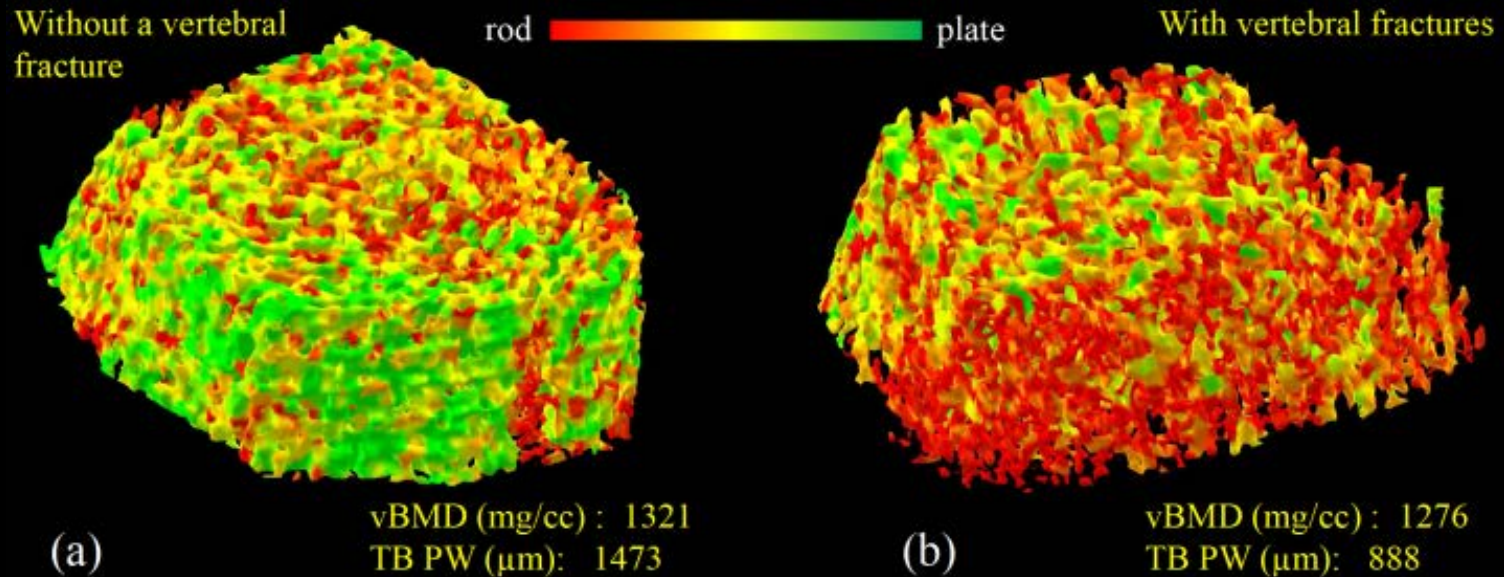
Color-coded illustration of trabecular bone (TB) plate/rod classification for a IBDS female control (a) and an age-similar, sex- and BMI-matched patient on continuous treatment with an SSRI (b), and another age-similar, sex- and BMI-matched patient with confirmed diagnosis of CF (c). The healthy female (a) has more TB plates (green) as compared to the two patient participants. Between the two patients, the CF patient (c) has some signs of heterogeneous bone loss.

Study 3

Aim: To determine bone structural differences in fracture vs non0-fracture groups

Bone Structural Differences in vertebral Fracture vs Non-Fracture Groups

- 30 patients (13 male) with COPD GOLD status between 1 and 4
- age: 70.6 ± 8.1 years BMI: 27.5 ± 4.2
- 23 patients with at one vertebral fracture



- The patient without a vertebral fracture has $\approx 50\%$ more Tb plates (green)
- The difference in Tb volumetric BMD between the two male patients is only 3.5%

Bone Structural Differences in vertebral Fracture vs Non-Fracture Groups

- 30 patients (13 male) with COPD GOLD status between 1 and 4
- age: 70.6±8.1 years BMI: 27.5±4.2
- 23 patients with at one vertebral fracture

	CB Th (μm)	CB Poro	v-BMD (mg/cc)	pBMD (mg/cc)	tBMD (mg/cc)	TB NA (mm^2/mm^3)	TB PW (μm)	TB Th (μm)	TB Sp (μm)
Non-fracture	1862	0.20	1101	818	222	0.47	995.0	120.5	513.5
Fracture	1745	0.21	1088	723	181	0.41	889.3	121.6	571.6
Difference	6.3%	-6.4%	1.2%	11.6%	18.3%	13.6%	10.6%	-0.9%	-11.3%
p-value	0.328	0.226	0.147	0.056	0.054	0.058	0.090	0.427	0.279

The difference (%) in MDCT-based bone measures between fracture (n = 23) and non-fracture (n = 7) groups of patients with COPD

Study 4

Aim: To determine the normative distribution of MDCT bone measures and their relationships with DXA

Normative Distribution of MDCT Bone Measures and their Relationships with DXA

- Healthy volunteers (N = 324) from the Iowa Bone Development Study
 - Age: 19.8 ± 0.7 years
 - 178 females and 146 males
 - Cb measures were computed over 14-16% of tibia, while Tb measures were computed over 4-6% of tibia with a 30% peel (Table 1)
 - Whole-body, hip, spine, and left-leg DXA areal BMD measures were obtained on a Hologic Discovery A model densitometer
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Normative Distribution of Bone Measures

<i>Variables</i>	<i>Males (n=146)</i>	<i>Females (n = 178)</i>
Scan-age (Y)	19.77 (0.74)	19.77 (0.69)
Height (cm)	180.2 (7.7)**	166.4 (6.9)
Weight (kg)	84.74 (19.90)**	70.64 (19.31)
BMI	26.05 (5.60)	25.44 (6.49)
<i>DXA aBMD</i>		
Whole-body	1.283 (0.099)**	1.165 (0.090)
Hip	1.174 (0.165)**	1.031 (0.132)
Spine	1.099 (0.119)**	1.054 (0.130)
Left leg	1.390 (0.125)**	1.205 (0.103)
<i>MDCT Cortical</i>		
Cb.poro	0.219 (0.022)**	0.205 (0.042)
Cb.Th (mm)	2.319 (0.269)**	2.006 (0.236)
<i>MDCT Trabecular</i>		
Tb.vBMD (mg/cc)	1182.9 (27.7)**	1164.4 (32.1)
Tb.tBMD (mg/cc)	360.4 (74.2)**	312.1 (86.3)
Tb.pBMD (mg/cc)	1005.0 (103.1)**	928.2 (120.9)
Tb.NA (mm ² /mm ³)	0.063 (0.013)**	0.050 (0.013)
Tb.PW (μm)	1375.7 (300.2)**	1211.0 (315.9)
Tb.Th (μm)	173.2 (24.9)**	161.6 (23.8)
Tb.Sp (μm)	398.0 (63.9)**	439.6 (85.1)

Correlations for MDCT Cortical and Trabecular Bone Outcomes with DXA Areal BMD

Variable	<u>Female</u>								
	Cb.poro	Cb.Th	Tb.vBMD	Tb.tBMD	Tb.pBMD	Tb.NA	Tb.PW	Tb.Th	Tb.Sp
Whole-body	-0.08	0.39**	0.64**	0.61**	0.58**	0.64**	0.61**	0.53**	-0.57*
Hip	-0.06	0.44**	0.61**	0.60**	0.56**	0.63**	0.58**	0.50**	-0.54*
Spline	-0.08	0.29**	0.49**	0.46**	0.40**	0.46**	0.44**	0.36**	-0.43*
Left leg	-0.07	0.60**	0.64**	0.65**	0.64**	0.69**	0.65**	0.61**	-0.57*

Variable	<u>Male</u>								
	Cb.poro	Cb.Th	Tb.vBMD	Tb.tBMD	Tb.pBMD	Tb.NA	Tb.PW	Tb.Th	Tb.Sp
Whole-body	0.20*	0.41**	0.48**	0.48**	0.41**	0.55**	0.40**	0.36**	-0.50*
Hip	0.08	0.41**	0.55**	0.54**	0.48**	0.59**	0.48**	0.43**	-0.53*
Spline	0.17*	0.29**	0.34**	0.34**	0.30**	0.37**	0.26**	0.25**	-0.34*
Left leg	0.18*	0.51**	0.57**	0.54**	0.52**	0.61**	0.52**	0.50**	-0.52*

Moderate correlations between MDCT and DXA outcomes suggest uniqueness of bone structural properties captured by MDCT measures as compared to DXA

Conclusions

- Advanced quantitative characterization of bone micro-architecture are suited for medical imaging research and clinical studies.
 - Multi-detector CT is a potential imaging modality for *in vivo* assessment of human trabecular bone micro-architecture
 - Bone data from multiple MDCT scanners can be used in large studies after adjustment using proper calibration equation
 - Normative distributions of MDCT bone measures are define disease groups
 - Low to moderate correlation for MDCT bone measures with DXA outcomes suggests uniqueness of MDCT measures
 - Bone structural differences in different human groups may provide new insights of the etiology of bone diseases
 - MDCT bone measures may be useful to predict fracture risk
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Steven M. Levy, Eric Hoffman, Trudy L. Burns, Richard Shields, Chadi A. Calarge, James C. Torner, Laurie M. McCormick, Ravi Regatte, X. Edward Guo, Felix W. Wehrli, Elizabeth Regan, Alexadro Comellas

Scientists/Post-doctoral Fellows/Engineers

Guoyuan Liang, Duan Hong, Subhadip Basu, Jamuna Kanta Singh, Ryan Amelon, Zhiyun Gao

Graduate Students

Zhiyun Gao, Yinxiao Liu, Ziyue Xu, Yan Xu, Cheng Li
Dakai Jin, Cheng Chen, Xiaoliu Zhang, Syed Nadeem Ahmed,
Indranil Guha

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